

# Mathematics of X-ray Computed Tomography: Just Enough Physics and Continuous Theory

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# (Rough) Outline

## Lecture 1 – Monday 5<sup>th</sup> January

- What is tomography? Just enough physics
- A splash of theory on the Radon transform and Filtered Backprojection

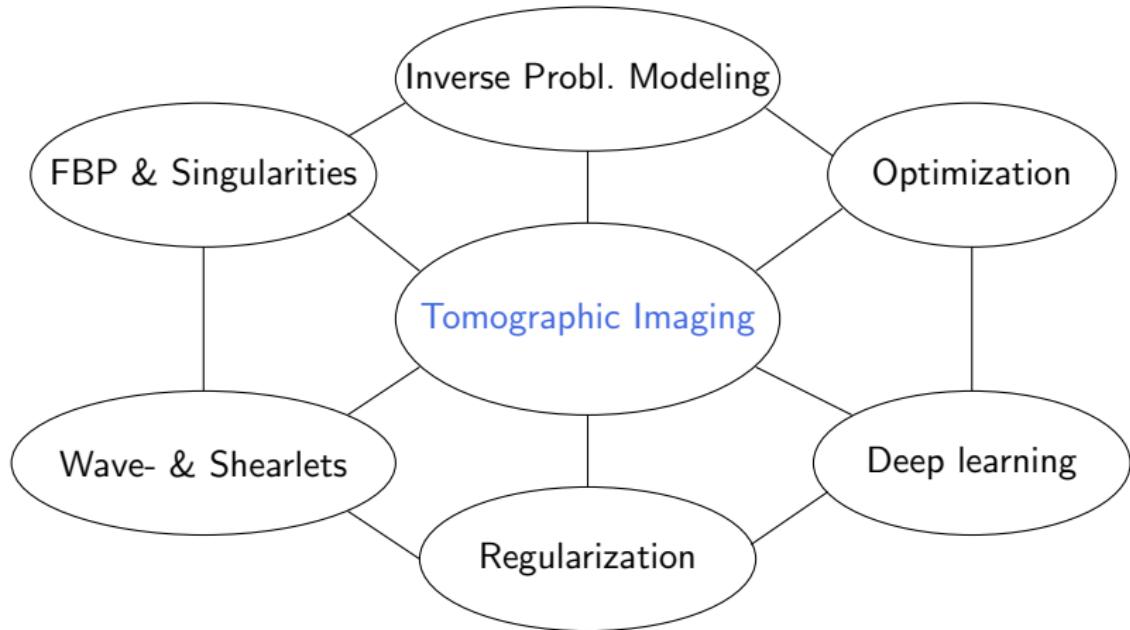
## Lecture 2 – Tuesday 6<sup>th</sup> January

- Regularisation methods to solve (tomographic) inverse problems
- A very fast wavelet tour (of signal processing)

## Lecture 3 – Wednesday 7<sup>th</sup> January

- Nods to convex optimization
- Short introduction to learned reconstruction methods

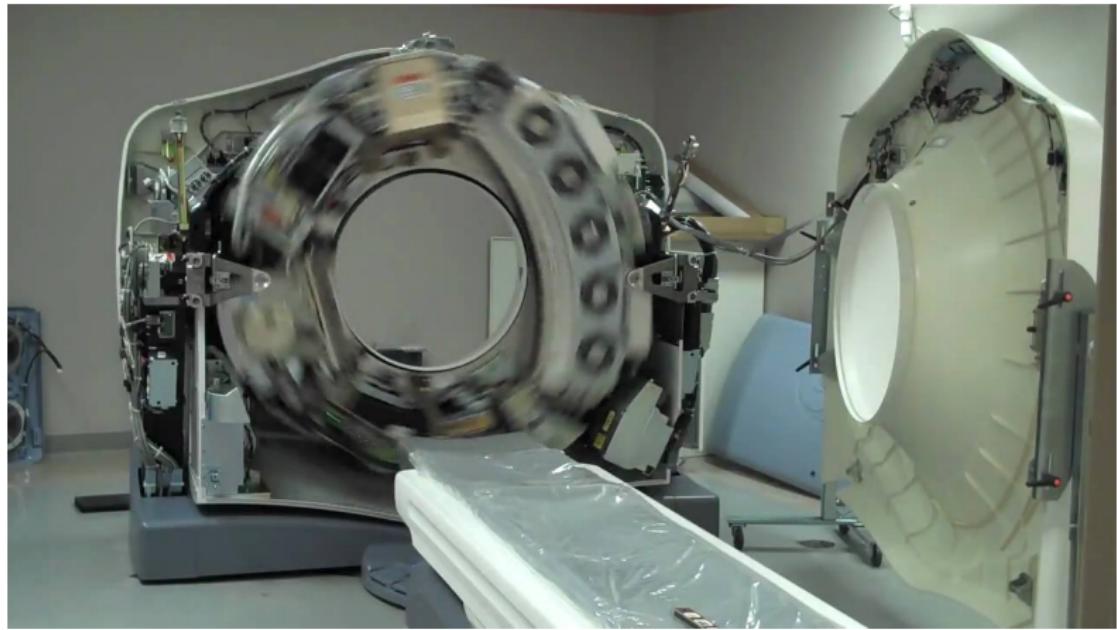
## (Rough) Outline But With a Drawing



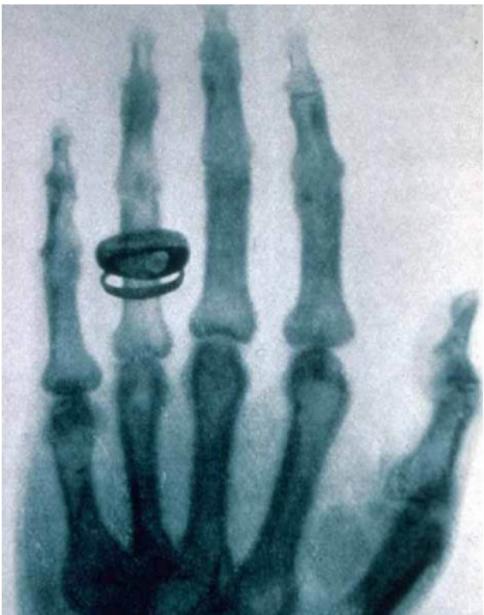
# Modern CT Scanners



# Modern CT Scanners: Inside



## The Story Begins With Röntgen's Discovery of X-rays

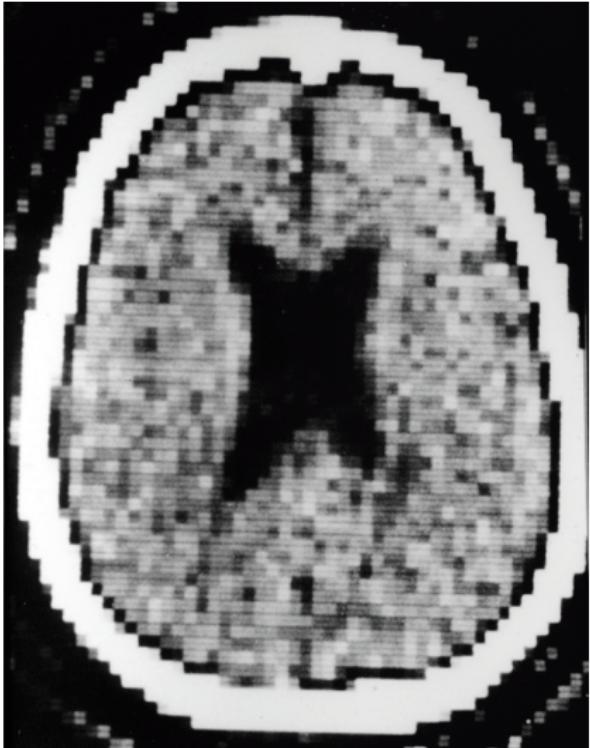


1895: Wilhelm Conrad Röntgen discovers X-rays

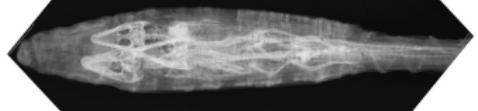
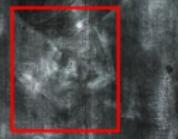
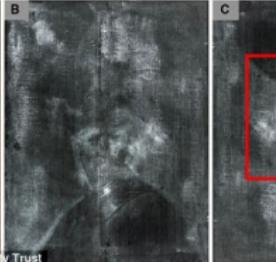
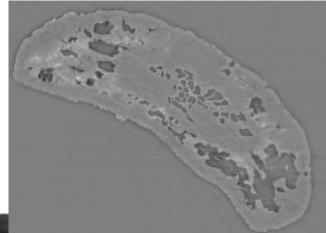
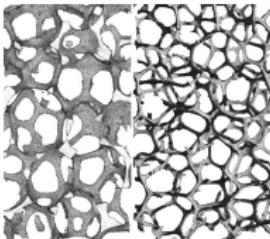
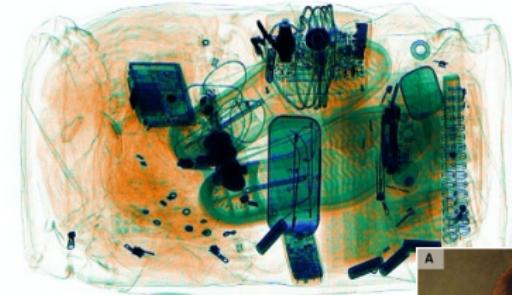
1901: Röntgen is awarded the Nobel Prize in Physics

## Several Decades Later ...

1979: Godfrey Hounsfield (top) and Allan McLeod Cormack receive the Nobel prize for developing X-ray tomography.



# Nowadays: Deluge of Applications



# What is Computed Tomography?

**Tomography:** derives from *tomos* (a section or slice) and *graphos* (to describe)

CT is a [non-invasive](#) device that provides information about the inside of an object by taking measurements from the outside ([indirect information](#)).



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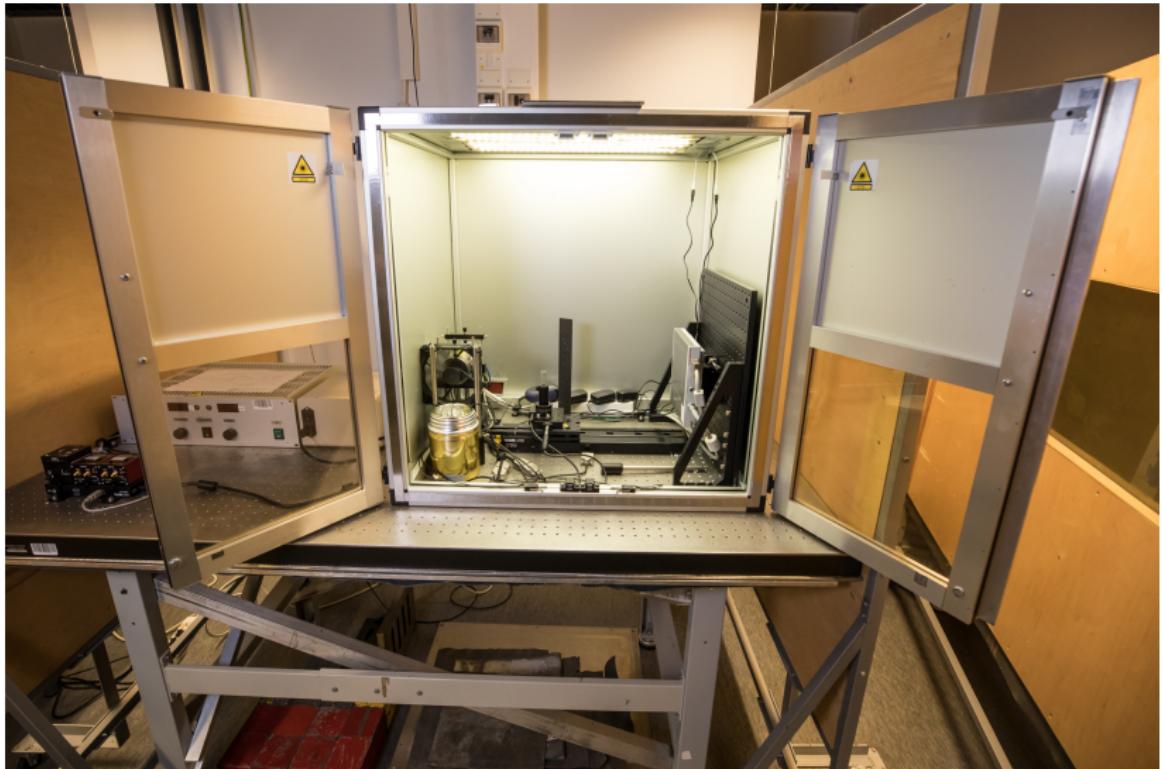
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## At the core:

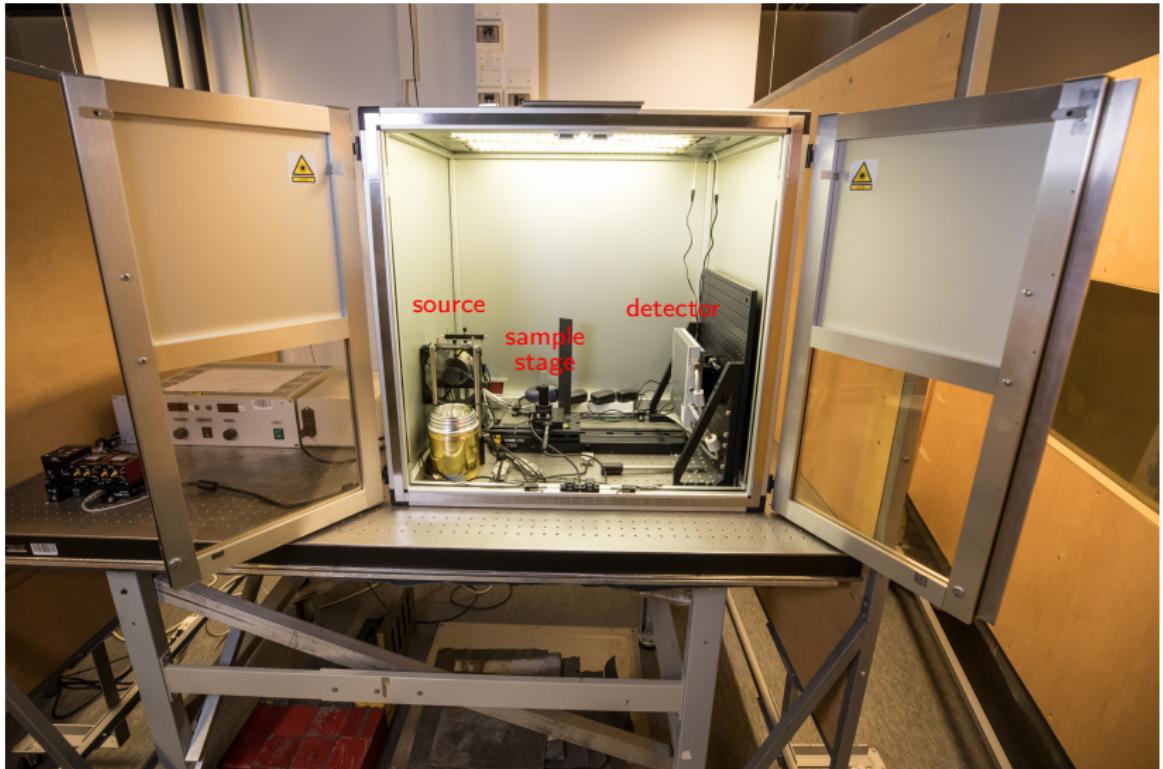
- Measurements are taken exploiting the transmission of waves or particles (e.g., X-rays)
- The intensity of particles transmission is attenuated by the material through which they travel

## In Practice: Experimental Imaging Setup



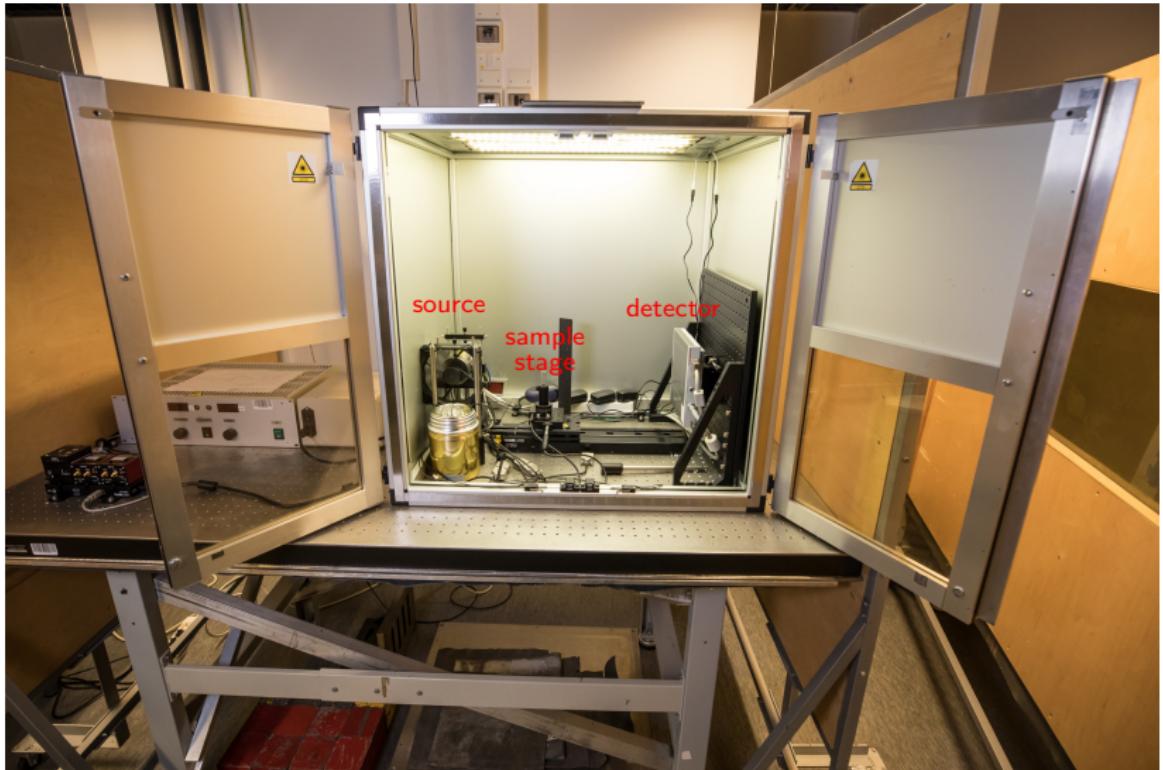
$\mu$ CT system at University of Helsinki

## In Practice: Experimental Imaging Setup



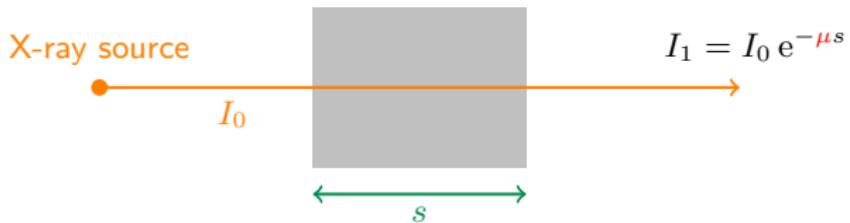
Primary components of  $\mu$ CT system: source, target, detector

## In Practice: Experimental Imaging Setup



Source emits X-rays → passing through the target → measured by detector

## Toy Example: A Line Inside Homogeneous Matter

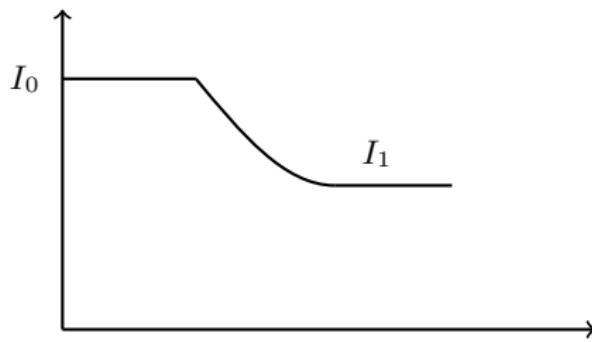
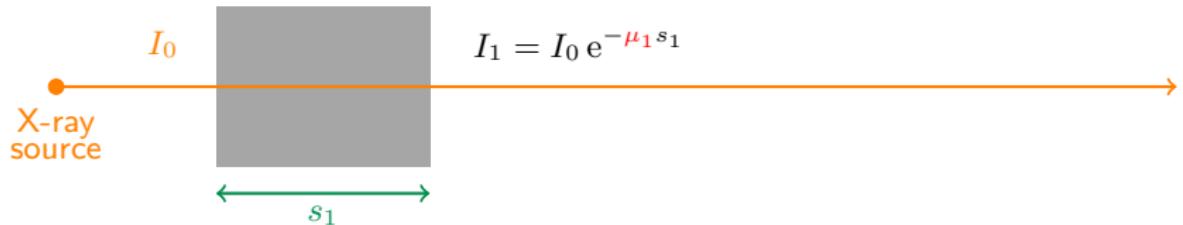


$I_0$ : initial intensity of the X-ray

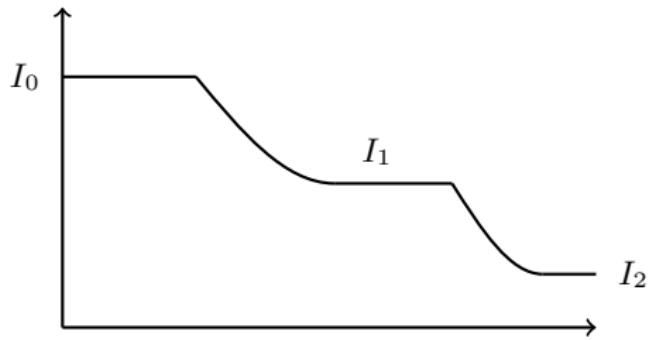
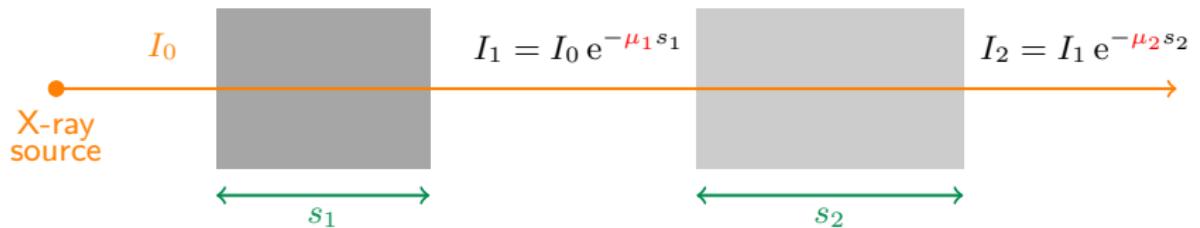
$s$ : length of the path of the X-ray inside the object (particles are assumed to more or less travel in straight lines)

$\mu > 0$ : X-ray attenuation coefficient

## Toy Example: Two Homogeneous Blocks



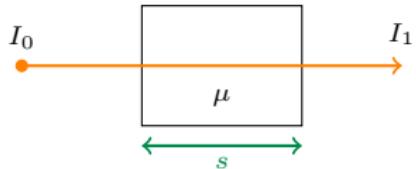
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# Absorption in the Target: the Beer-Lambert Law

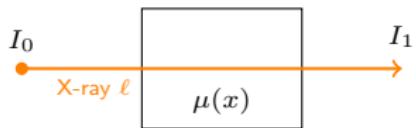
**Homogeneous material:**

$$I_1 = I_0 e^{-\mu s}$$



**Non-homogeneous material:**

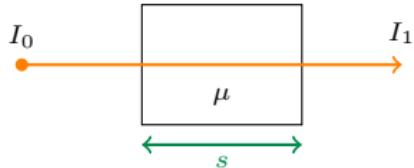
$$I_1 = I_0 e^{-\int_{\ell} \mu(x) dx}$$



# Absorption in the Target: Energy Dependence

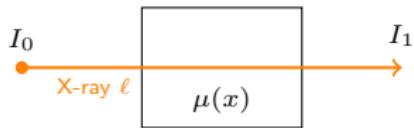
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**Non-homogeneous material:**

$$I_1 = I_0 e^{- \int_{\ell} \mu(x) dx}$$



In reality, to accurately describe the physical process an **energy-dependent non-linear integral** model would be necessary:

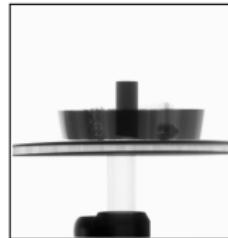
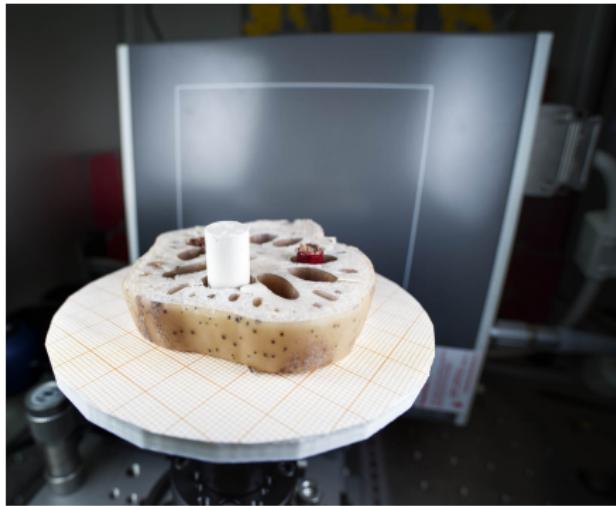
$$I_1 = \int I_0(E) e^{- \int_{\ell} \mu(E, x) dx} dE$$

Usually, this energy-dependence is neglected and an effective absorption coefficient  $\mu_{\text{eff}}(x)$  is assumed.

## Imaging at the Detector

The detector measures a resulting X-ray projection image:

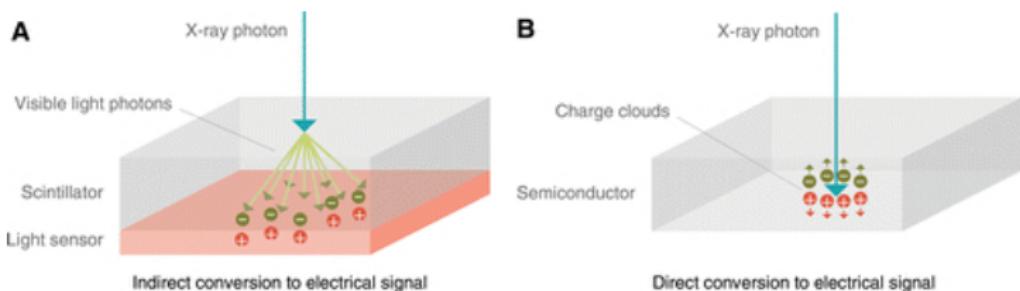
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## Imaging at the Detector

The detector measures a resulting X-ray projection image:

- The most common energy integrating detectors (EIDs) provide a monochromatic image
- Photon counting detectors (PCDs) can detect photons of different energies and allow for multi-energy X-ray (nonlinear)



[Image credits: Willemink et al., Radiology, 2018]

## Transforming the Measurement for the Inverse Problem

The Beer-Lambert law connects the initial and final intensities of an X-ray:

$$I_1 = I_0 e^{-\int_{\ell} \mu(x) dx} \iff -\log\left(\frac{I_1}{I_0}\right) = \int_{\ell} \mu(x) dx$$

where  $-\log(I_1/I_0)$  models the total attenuated energy according the attenuation along the path  $\ell$ .

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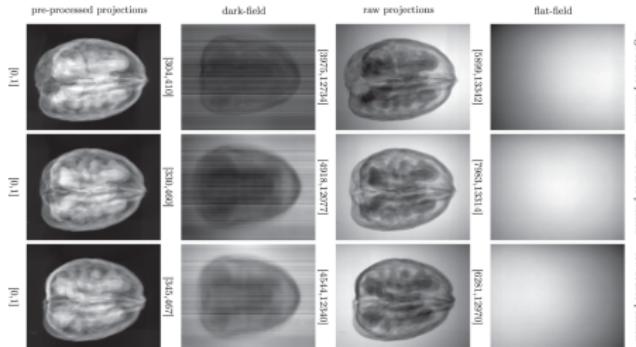
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Before obtaining processed measurements, need to compensate “detector noise”:

- **Dark-field** recorded with source off: detector offset count
- **Flat-field** with source on: the beam profile



[Der Sarkissian et al., Scientific Data, 2019]

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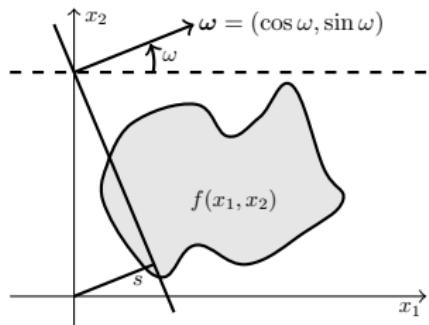
As a result, during a tomographic scan:

- $I_0$  is known from calibration and  $I_1$  from measurements
- $I_1$  is measured along many lines  $\ell_{(\omega,s)}$  to get many line integral values through the object
- The intensity  $I_1$  is called the *transmission*, while the corresponding  $-\log(I_1/I_0)$  is called absorption or **projection**, and a collection of projections is called a **sinogram**

## Beer-Lambert Law and Radon Transform

The problem of recovering the attenuation function (linearised measurement) can be mathematically modelled by the **Radon transform**, which can be understood as an integration of the function  $f : \mathbb{R}^2 \rightarrow \mathbb{R}_+$  over lines.

Through the identifications  $f(\mathbf{x}) = \mu(\mathbf{x})$  and  $\mathcal{R}(f) = -\log(I_1/I_0)$ , the Beer-Lambert law is connected to the **Radon transform**:

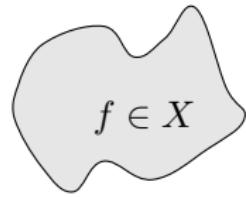


$$\begin{aligned}\mathcal{R}(f)(\omega, s) &= \int_{-\infty}^{\infty} f(s\omega + \tau\omega^\perp) d\tau \\ &= \int_{\ell(\omega, s)} f(\mathbf{x}) d\mathbf{x},\end{aligned}$$

where  $\ell = \ell(\omega, s) = \{\mathbf{x} \in \mathbb{R}^2 : \mathbf{x} = s\omega + \tau\omega^\perp, \tau \in \mathbb{R}\}$  with  $\omega = (\cos(\omega), \sin(\omega))$  and  $(\omega, s) \in S^1 \times \mathbb{R}$ .

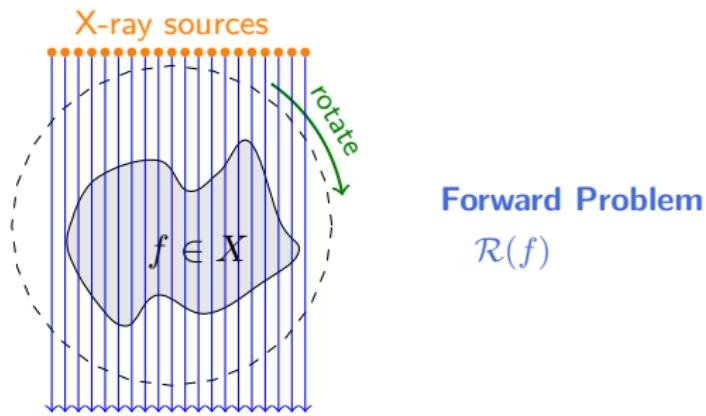
## In Practice: How to Formulate CT as a Mathematical Problem

- We aim at imaging a target (e.g., human chest)  $f \in X = L^2(\Omega)$  with  $f : \mathbb{R}^d \rightarrow \mathbb{R}_+$  in a bounded domain  $\Omega \in \mathbb{R}^d$ ,  $d = 2, 3$ .



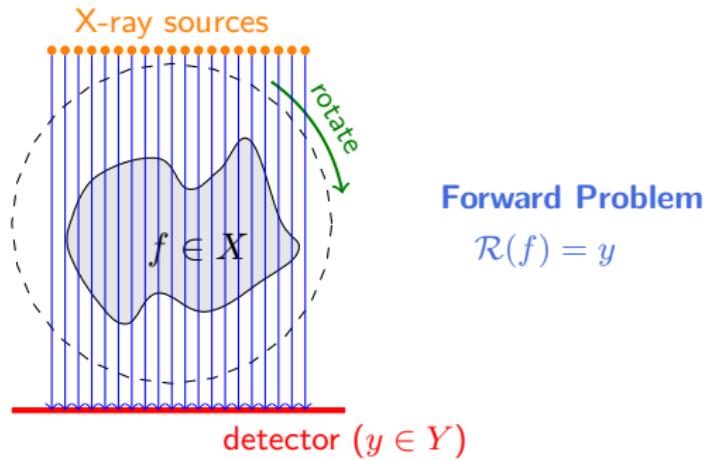
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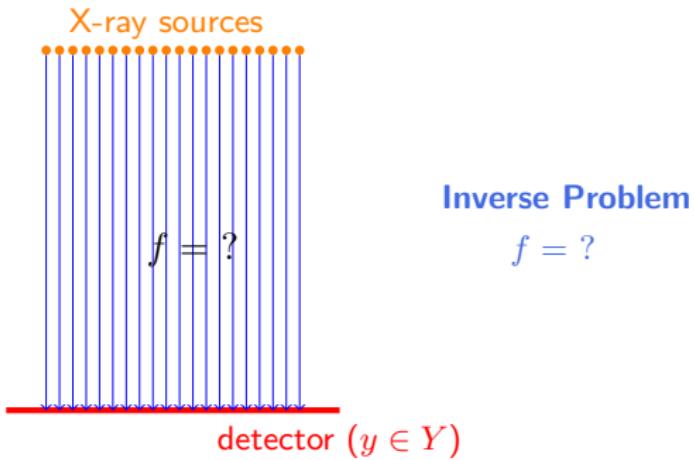
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- Reconstructing  $f$  from the measured data  $y$  is then consequently the **inverse problem**.



# The Basic Linear Inverse Problem

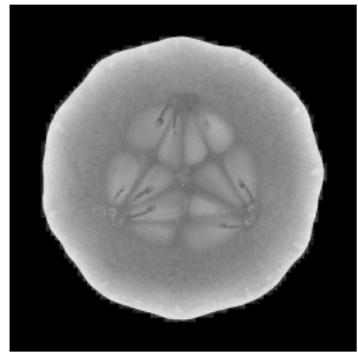
The forward model can be stated as:

$$Af = y^\delta$$

where:

$A : X \rightarrow Y$  The linear forward operator  
(defining the *scanning geometry*)

$f \in X$  The unknown/quantity of interest  
(*linearised attenuation coefficient*)



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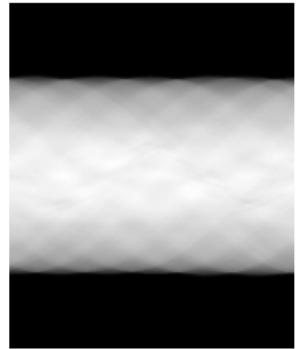
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measurement data

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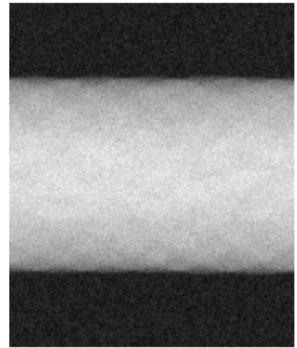
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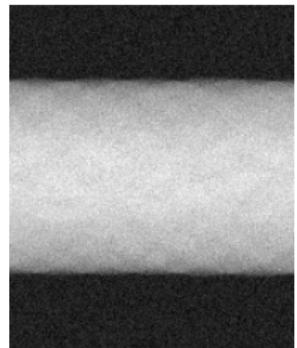
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## Inverse problem

Given noisy measurements  $y^\delta$ , determine  $f$ .

## III-Posedness and Hadamard's Conditions



The problem

Given  $y^\delta$ , determine  $f$  with  $Af = y^\delta$

is well-posed if the following conditions hold true [Hadamard, 1903]:

1. A solution exists ([surjectivity](#))
2. The solution is unique ([injectivity](#))
3. The solution depends continuously on the input ([stability](#))

If one of these conditions fails, the problem is said [ill-posed](#).

## A splash of continuous theory: Radon transform

Recall the the Radon transform

$$y(\omega, s) = \mathcal{R}(f)(\omega, s) = \int_{\ell(\omega, s)} f(\mathbf{x}) \, d\mathbf{x}$$

- It is dependent on an **angle** on the unit circle  $\omega \in (0, 2\pi]$ , with  $\omega = (\cos(\omega), \sin(\omega))$ , and a **signed distance**  $s \in \mathbb{R}$ .
- $d\mathbf{x}$  denotes the one-dimensional (Lebesgue) measure along the line  $\ell(\omega, s) = \{\mathbf{x} \in \mathbb{R}^2 : \mathbf{x} \cdot \omega = s\}$ , i.e., we only integrate over single lines for each  $\omega$  and  $s$ !
- The measurement  $y = \mathcal{R}(f)$  is a function defined on the parametrization of the infinite unit cylinder in  $\mathbb{R}^3$ :

$$C^2 = \{(\omega, s) : \omega \in [0, 2\pi), s \in \mathbb{R}\}.$$

- Notice that  $\mathcal{R}(f)(\omega, s) = \mathcal{R}(f)(-\omega, -s)$ , so we can take  $\omega \in (0, \pi]$ .

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Integrating over lines for each angle  $\omega = (\cos(\omega), \sin(\omega))$  for  $\omega \in (0, \pi]$  results in the sinogram.

## Boundedness of the Radon Transform

Given a linear operator  $\mathcal{A} : X \rightarrow Y$  between two Banach/Hilbert spaces, we say that the operator is **bounded**, if there exists a constant  $C > 0$  such that

$$\|\mathcal{A}f\|_Y \leq C\|f\|_X, \quad \text{for all } f \in X.$$

The smallest such  $C$  is the operator norm  $\|\mathcal{A}\|_{\text{op}} = \|\mathcal{A}\|_{X \rightarrow Y} = C$ . In particular, a **bounded linear operator is continuous**.

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### Theorem

Let  $\mathcal{R}$  be the Radon transform,  $\Omega_1 \subset \mathbb{R}^2$  a bounded set and  $\text{supp}(f) \subset \Omega_1$ , so that the integration reduces to  $\ell(\omega, s) \cap \Omega_1$ . Then  $\mathcal{R}$  is a **bounded linear operator** from  $L^2(\Omega_1)$  to  $L^2(C^2)$ . That is,  $\exists c > 0$  such that:

$$\|\mathcal{R}f\|_{L^2(C^2)} \leq c\|f\|_{L^2(\Omega_1)}, \quad \forall f \in L^2(\mathbb{R}^2).$$

## The Adjoint Operator or Backprojection

The Radon transform defines the forward operator  $X \rightarrow Y$  (image to measurement), **for reconstruction we also need a mapping from  $Y \rightarrow X$  (measurement to image)**.

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For that purpose, we will first use the **adjoint operator**  $\mathcal{R}^*$ , which is defined through the inner product by the relationship:

$$\langle \mathcal{R}g, h \rangle_Y = \langle g, \mathcal{R}^*h \rangle_X, \quad \text{for all } g \in X, h \in Y,$$

where the inner product is the inner product in  $L^2(\Omega)$  (where our image  $f$  is defined), with  $\Omega \subset \mathbb{R}^2$ :

$$\langle g, h \rangle_{L^2(\Omega)} = \int_{\Omega} g(z)h(z)dz.$$

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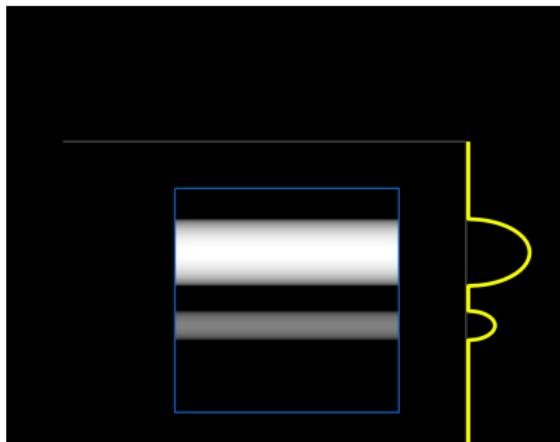
With this we can define the adjoint operator for the Radon transform, commonly referred to as **backprojection**.

## The Adjoint Operator or Backprojection

For the functions  $f(\mathbf{x})$ , with  $\mathbf{x} \in \Omega \subset \mathbb{R}^2$ , and  $y(\omega, s)$  with  $(\omega, s) \in S^1 \times \mathbb{R}$ , the adjoint  $\mathcal{R}^*$  (called **backprojection**) of the Radon transform is given by:

$$(\mathcal{R}^* y)(\mathbf{x}) = \int_0^\pi y(\omega, \mathbf{x} \cdot \omega) d\omega$$

The adjoint  $\mathcal{R}^*$  is linear. It can be understood as taking all lines that go through  $\mathbf{x}$  and averaging their projection values:



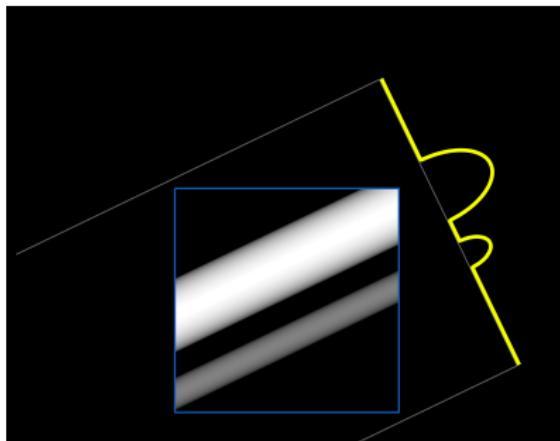
[Image credits: Samuli Siltanen]

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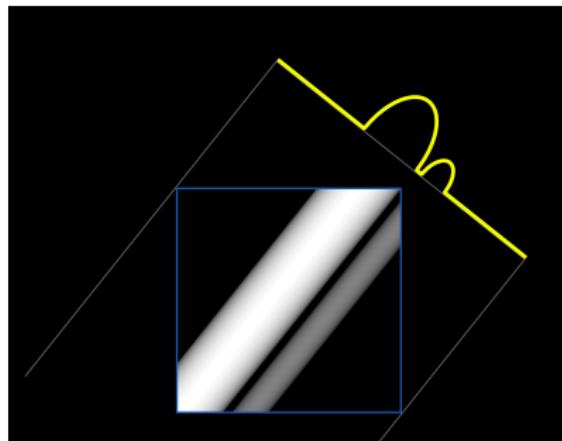
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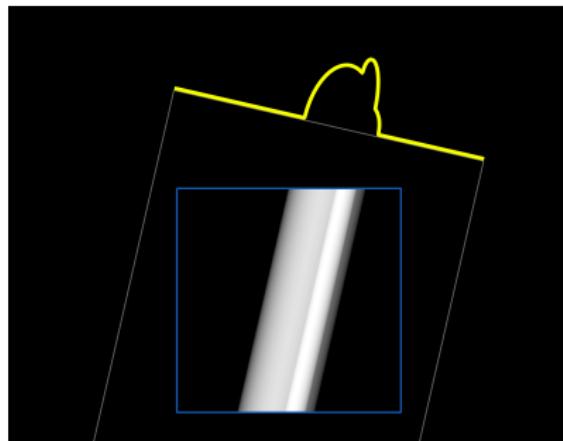
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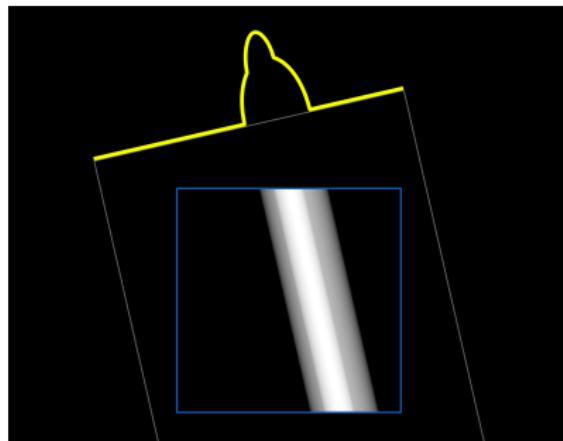
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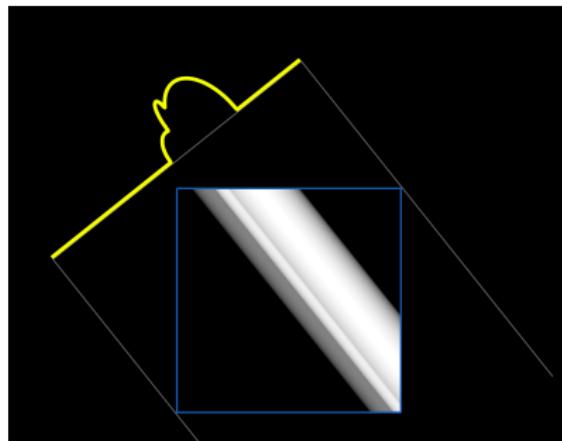
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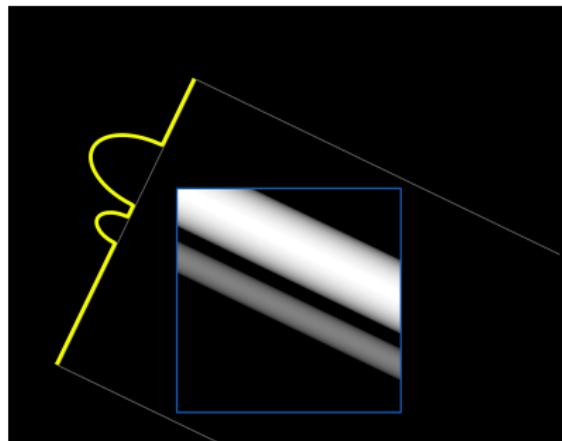
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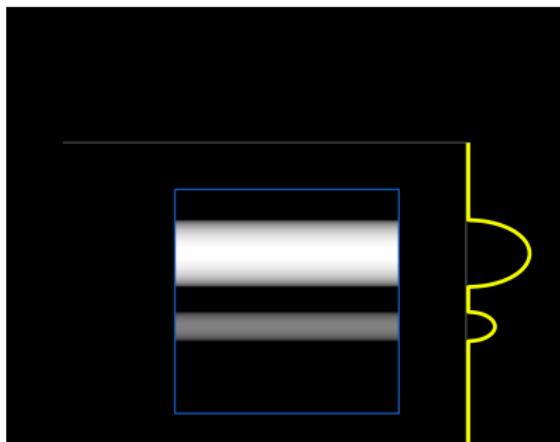
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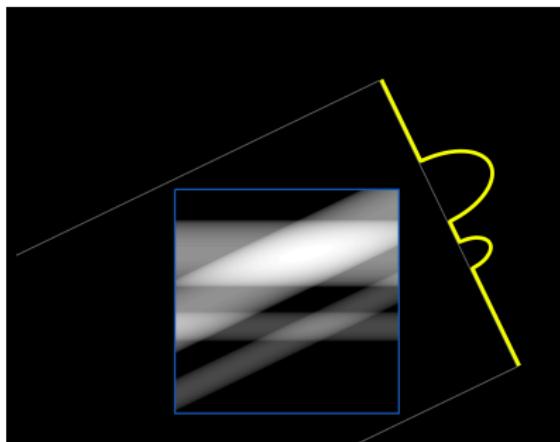
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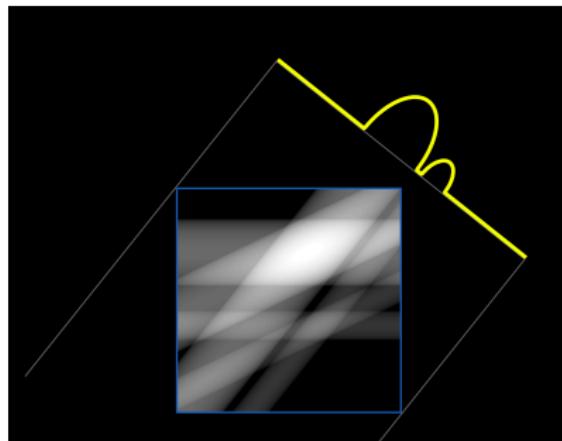
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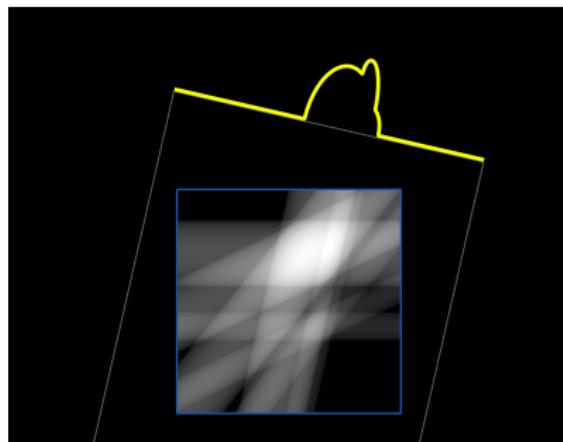
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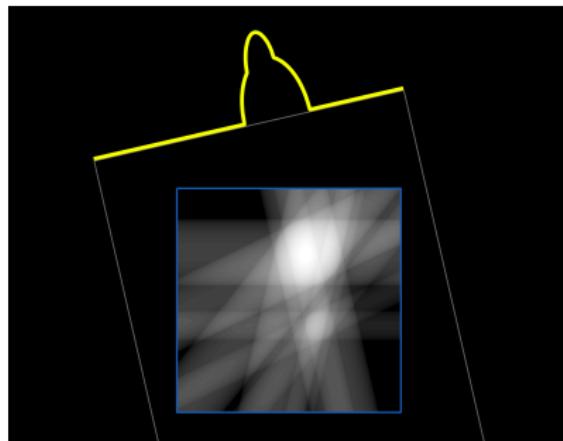
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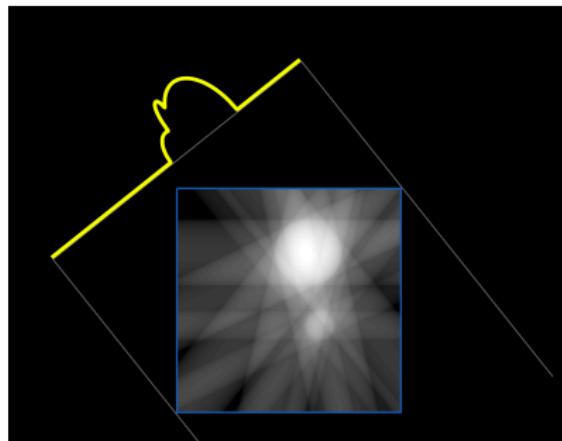
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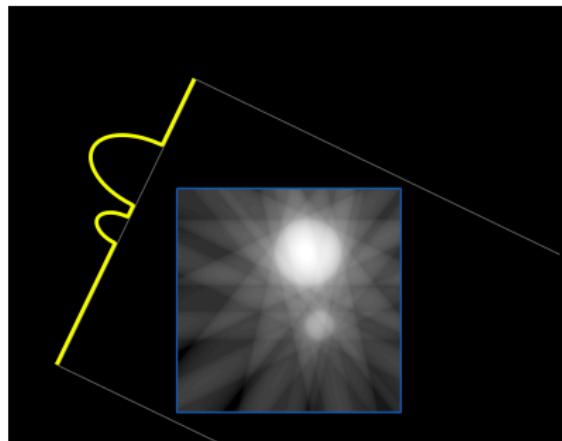
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[Image credits: Samuli Siltanen]

## Regularity of the Radon Transform

Theorem [2.10 with  $n = 2$ ,  $\alpha = 0$ , Natterer & Wübbeling 2001]

Let  $f \in L^2(\Omega_1)$ , then there exist two constants  $c, c' > 0$  such that

$$c\|f\|_{L^2(\Omega_1)} \leq \|\mathcal{R}f\|_{H^{1/2}(C^2)} \leq c'\|f\|_{L^2(\Omega_1)}.$$

Roughly speaking, the Radon transform is a continuous linear operator from  $L^2(\Omega_1)$  to  $H^{1/2}(C^2)$  and hence  $\mathcal{R}f$  is smoother than  $f$  by half a derivative.

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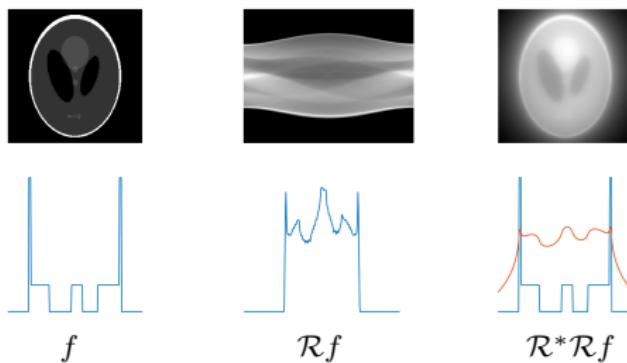
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A similar result holds for the backprojection, which means that the projection of  $f$  followed by a backprojection, i.e.  $\mathcal{R}^*\mathcal{R}f$ , smooths  $f$  by a full derivative.



### III-Posedness of the Radon Transform

✓ **Injectivity.** We have the following result:

#### Theorem

Let  $S_0 \subset S^1$  be a set of **infinite** many directions and let  $f \in L^2(\Omega_1)$ . If  $(\mathcal{R}f)(\omega, \cdot) = 0$  for every  $\omega \in S_0$ , then  $f = 0$ .

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However:

#### Caveat!

This is **not** true for **finitely** many directions!! Which means, this does not hold in the discrete case!

### III-Posedness of the Radon Transform

- ✓ **Injectivity.** The infinite dimensional Radon transform is injective.
- ✗ **Surjectivity.** The range of  $\mathcal{R}$  is an **infinite** dimensional proper subspace (i.e.,  $H^{1/2}(C^2)$ ) of  $L^2(C^2)$  (see again Theorem 2.10 in [Natterer & Wübbeling 2001]).

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Moreover:

#### Corollary

The Radon transform is a **compact operator** with infinite-dimensional range and hence it has an open range in  $L^2(C^2)$ .

- ✗ **Stability.** The range of the Radon transform is open so there is **no stability**.

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- ✗ **Surjectivity.** The Range is a proper subspace (i.e.,  $H^{1/2}(C^2)$ ) of  $L^2(C^2)$  and hence the Radon transform is **not surjective**.
- ✗ **Stability.** The range of the Radon transform is open so there is **no stability**.

# Can We Invert the Radon Transform?



Johann Radon (1887-1956)

How to reconstruct a function from its line integrals:

$$f(P) = -\frac{1}{\pi} \int_0^\infty \frac{d\bar{F}_p(q)}{q}$$

SITZUNG VOM 30. APRIL 1917.

Über die Bestimmung von Funktionen durch ihre Integralwerte längs gewisser Mannigfaltigkeiten.

Von

JOHANN RADON.

*Satz III: Der Wert von  $f$  ist durch  $F$  eindeutig bestimmt und lässt sich folgendermaßen berechnen:*

(III) 
$$f(P) = -\frac{1}{\pi} \int_0^\infty \frac{d\bar{F}_p(q)}{q}.$$

[from Johann Radon's 1917 Seminal Paper]

## Radon's Inversion Formula: Modern Version

Let  $f : \Omega \rightarrow \mathbb{R}$  and  $y = \mathcal{R}f$  then, for  $\mathbf{x} \in \Omega \subset \mathbb{R}^2$ ,  $f$  can be obtained as:

$$f(\mathbf{x}) = \frac{1}{4\pi^2} \int_0^\pi \int_{\mathbb{R}} \frac{\partial_s y(\boldsymbol{\omega}, s)}{\mathbf{x} \cdot \boldsymbol{\omega} - s} \, ds \, d\omega$$

with  $\boldsymbol{\omega} = (\cos(\omega), \sin(\omega))$ .

**Note:** Practical reconstructions are **not** directly based on this formulation. However, similar ingredients are found:

- Integration over  $s$  with a function  $(\mathbf{x} \cdot \boldsymbol{\omega} - s)^{-1} \rightsquigarrow \text{Convolution}$
- Integration over  $\omega \rightsquigarrow \text{Backprojection}$

## Convolution Theorem for the Radon Transform

Recall that given two functions  $h, k : \mathbb{R}^n \rightarrow \mathbb{R}$ :

$$(h * k)(\mathbf{u}) = \int_{\mathbb{R}^n} h(\mathbf{z})k(\mathbf{u} - \mathbf{z}) \, d\mathbf{z} = \int_{\mathbb{R}^n} h(\mathbf{u} - \mathbf{z})k(\mathbf{z}) \, d\mathbf{z}$$

The convolution theorem establishes a connection to the Fourier transform:

$$\mathcal{F}(h * k)(\xi) = \hat{h}(\xi)\hat{k}(\xi)$$

Convolution in image space = Multiplication in Fourier space

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In fact, we can use convolutions to establish a connection between backprojected data and image space.

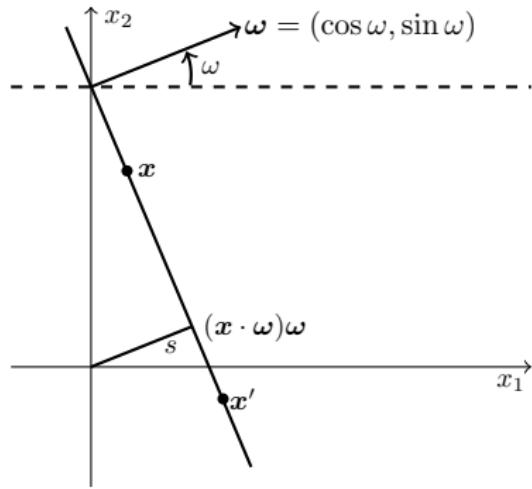
### Radon Convolution Theorem

Let  $v : C^2 \rightarrow \mathbb{R}$  and  $f : \Omega \rightarrow \mathbb{R}$ , then we have:

$$(\mathcal{R}^* v) * f = \mathcal{R}^*(v * \mathcal{R}f)$$

Conv. with BP kernel in image space = BP of conv. in data space

## Filtered Backprojection – Part I



First of all, notice that for each  $z \in \mathbb{R}^2$ , we have:

$$\begin{aligned} \exists \tau \in \mathbb{R} \text{ s.t. } (\mathbf{x} \cdot \omega)\omega + \tau\omega^\perp &= \mathbf{x}' \\ \Rightarrow \exists t \in \mathbb{R} \text{ s.t. } \mathbf{x} + t\omega^\perp &= \mathbf{x}' \end{aligned}$$

Then, let's start by computing  $\mathcal{R}^* \mathcal{R} f$ :

$$\begin{aligned} \mathcal{R}^* \mathcal{R} f(\mathbf{x}) &= \int_0^\pi \mathcal{R} f(\omega, \mathbf{x} \cdot \omega) d\omega = \int_0^\pi \int_{-\infty}^\infty f((\mathbf{x} \cdot \omega)\omega + \tau\omega^\perp) d\tau d\omega \\ &= \int_0^\pi \int_{-\infty}^\infty f(\mathbf{x} + t\omega^\perp) dt d\omega \end{aligned}$$

## Filtered Backprojection – Part II

Next, by using polar coordinates we get:

$$\begin{aligned}\mathcal{R}^* \mathcal{R} f(\mathbf{x}) &= \int_0^\pi \int_{-\infty}^\infty f(\mathbf{x} + t\omega^\perp) dt d\omega \\ &= \int_0^{2\pi} \int_0^\infty \frac{f(\mathbf{x} + t\omega^\perp)}{t} t dt d\omega = \int_{\mathbb{R}^2} \frac{f(\mathbf{x} + \mathbf{z})}{\|\mathbf{z}\|} d\mathbf{z}\end{aligned}$$

where  $\mathbf{z} = (z_1, z_2)$  with  $z_1 = -t \sin(\omega)$  and  $z_2 = t \cos(\omega)$ .

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Then, (with a trivial change of variables) we have:

$$\mathcal{R}^* \mathcal{R} f(\mathbf{x}) = \int_{\mathbb{R}^2} \frac{f(\mathbf{x} + \mathbf{z})}{\|\mathbf{z}\|} d\mathbf{z} = \int_{\mathbb{R}^2} \frac{f(\mathbf{z})}{\|\mathbf{x} - \mathbf{z}\|} d\mathbf{z} = (f * v)(\mathbf{x})$$

where  $v(\mathbf{x}) = \frac{1}{\|\mathbf{x}\|}$  and  $*$  denotes the convolution defined earlier.

## Filtered Backprojection – Part III

Now, notice that  $\hat{v}(\xi) = \frac{1}{|\xi|}$ , therefore by applying the Fourier transform we get:

$$\mathcal{F}(\mathcal{R}^* \mathcal{R} f)(\xi) = \mathcal{F}(f * v)(\xi) = \hat{f}(\xi) \hat{v}(\xi) = \frac{\hat{f}(\xi)}{|\xi|}$$

Finally, by multiplying both sides by  $|\xi|$  and applying the inverse Fourier transform, we end up with:

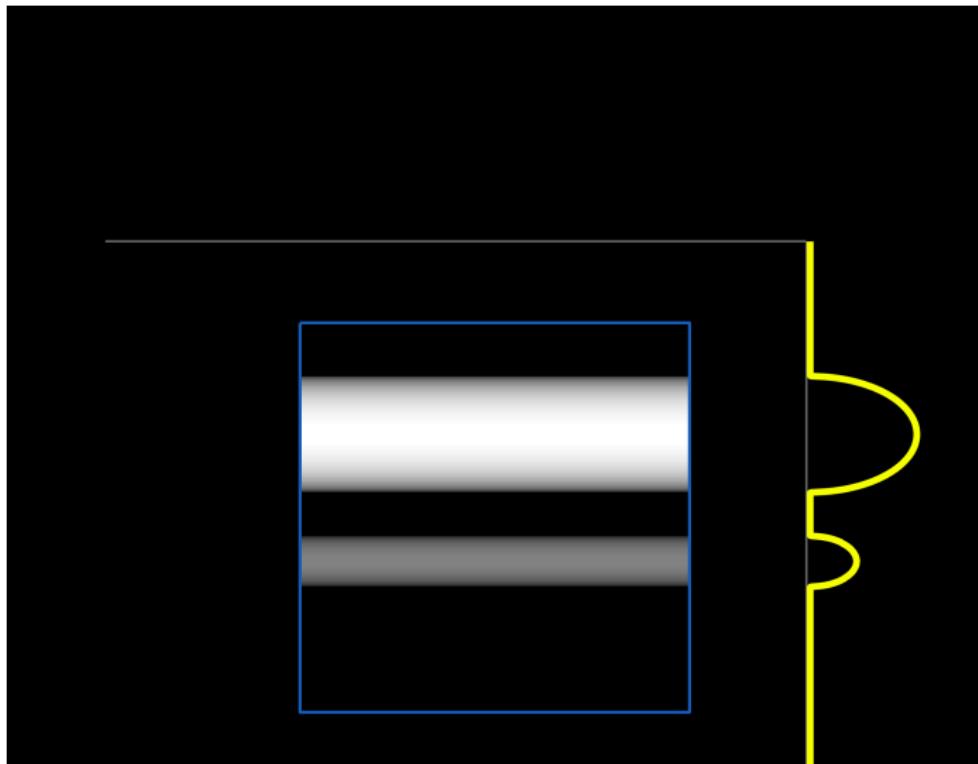
$$\Lambda \mathcal{R}^* \mathcal{R} f(\mathbf{x}) = \mathcal{F}^{-1}(|\xi| \mathcal{F}(\mathcal{R}^* \mathcal{R} f))(\mathbf{x}) = f(\mathbf{x}).$$

Hence,  $\Lambda \mathcal{R}^*$  acts as a left inverse for the Radon transform  $\mathcal{R}$ , where

$$\Lambda \mathcal{R}^* = \mathcal{F}^{-1} |\xi| \mathcal{F} \mathcal{R}^*$$

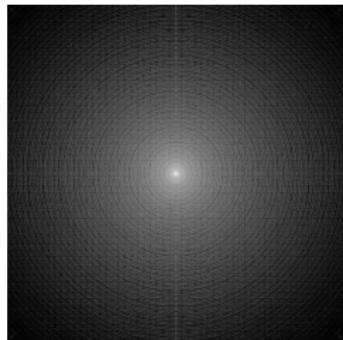
is the **Filtered Backprojection (FBP)** operator. Notice how the FBP operator leverages filtering on top of backprojecting the data: this allows to make singularities sharper.

# FBP as Numerical Implementation of Radon Reconstruction Formula



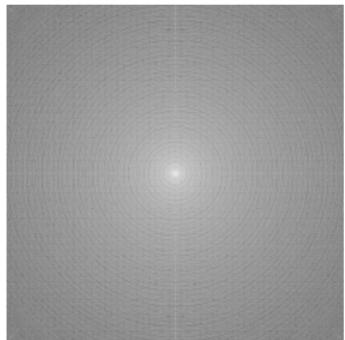
[Video credits: Samuli Siltanen]

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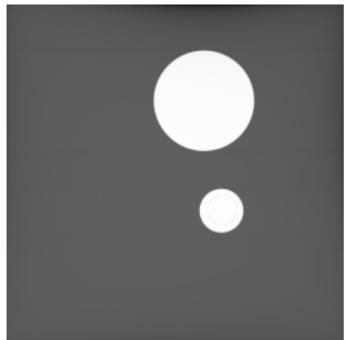
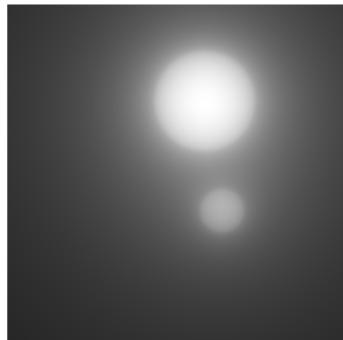


↑FFT

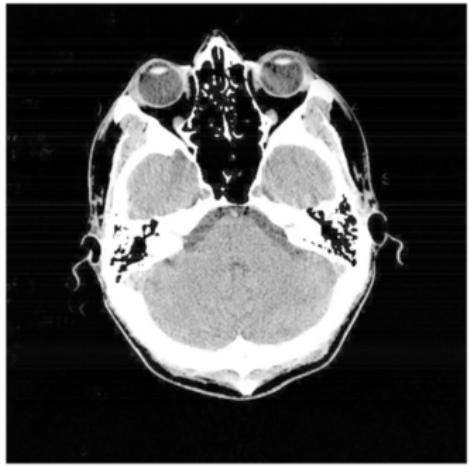
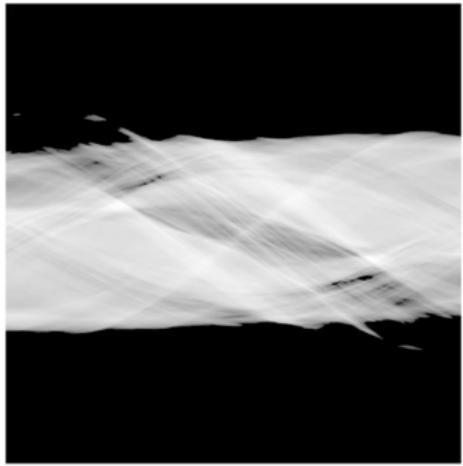
Multiplication with  
bandlimited function



↓IFFT

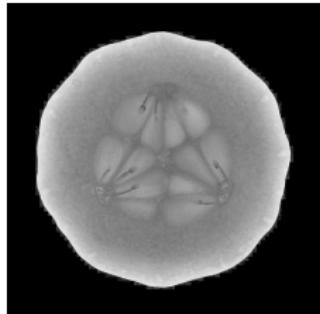


## Standard FBP In Action

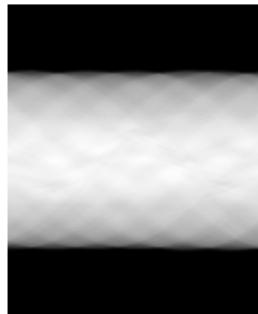


[Video credits: Samuli Siltanen]

# Why Do We Need Other Approaches Than FBP?



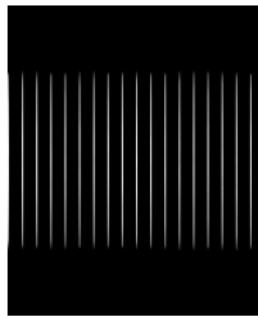
ground truth



Full angle data

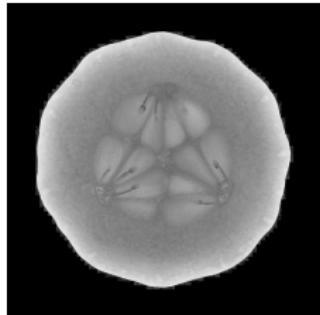


Limited-angle data

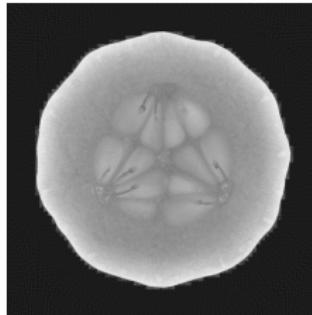


Sparse-angle data

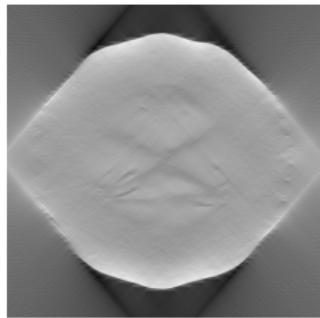
# Why Do We Need Other Approaches Than FBP?



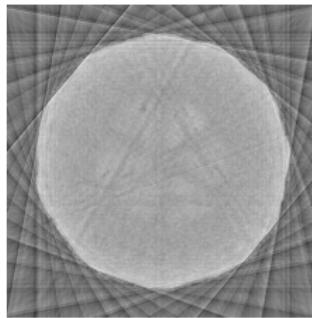
ground truth



FBP from full angle data



FBP from limited-angle data



FBP from sparse-angle data

## Why Do We Need Other Approaches Than FBP?

Actually, FBP works well when:

- comprehensive projection data are available
- the target is (assumed) static

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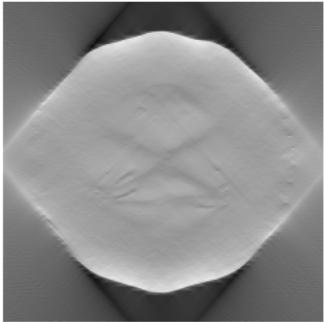
In many practical tomographic applications we wish to:

- lower the X-ray **radiation dose**       $\rightsquigarrow$       **Limited Data** tomography
- shorten the scanning **time**
- take into account **non-static** target       $\rightsquigarrow$       **Dynamic** tomography  
and time-dependance of measurements

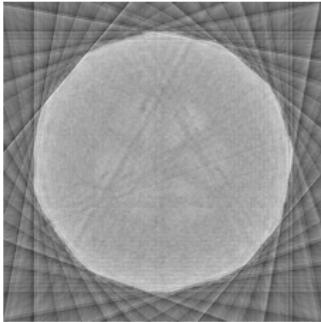
These are severely ill-posed problems and classical strategies like FBP not always suffice!

# Limited Data Tomography

**Notation:**  $\mathcal{R}_\Phi = \chi_{\Phi \times \mathbb{R}} \mathcal{R}$ , with  $\Phi \subset S^1$ , denotes both limited data operators.



$$\Phi = [\Gamma, \pi - \Gamma]$$



$$\Phi = [\omega_1 - \eta, \omega_1 + \eta] \cup \dots \cup [\omega_N - \eta, \omega_N + \eta]$$

- ▶ Parts of the edges, associated with specific directions, do **not** appear in the reconstruction
- ▶ Some additional edges appear, along specific lines (**streak artifacts**)
- ▶ Theoretical explanation via **microlocal analysis**  
(→ [MiniCourse 5 by Andras Vasy](#))

# Microlocal Analysis - Summary

Studies the singularities in functions (e.g., edges in images). Some tools:

- **singular support:** the set of points  $x_0$  near which  $f$  is not smooth;
- **wavefront set:**  $\text{WF}(f)$  set of pairs  $(x_0, \xi_0)$  of locations of jumps and their normal directions.

How does an operator  $A$  perturb the singularities of  $f$ ?

- **Pseudo-differential op.** ( $\Psi$ DO) preserve singularities:  $\text{WF}(Af) \subset \text{WF}(f)$
- **Fourier Integral op.** (FIO) can move singularities according to a canonical relation  $\text{WF}(Af) \subset C(\text{WF}(f))$

## Key examples:

- The Radon transform  $\mathcal{R}$  is a FIO (moves singularities along lines), but the normal operator  $\mathcal{R}^* \mathcal{R}$  is a elliptic  $\Psi$ DO
- For the limited data Radon transform  $\mathcal{R}_\Phi$ , theory of visibility principles (visible VS invisible singularities & streak artifacts)

## Summary & Outlook

What we learned today:

- ▶ Radon transform as mathematical model of tomographic imaging
- ▶ Filtered Backprojection
- ▶ Limited data tomography

What I do not have time to talk about:

- ▶ Other geometries (fan beam)
- ▶ Extension to 3D geometries (cone beam, helical beam)
- ▶ Alternative FBP formulas and how to implement them

Up next:

- ▶ Discretization of the problem
- ▶ A splash of regularization theory of inverse problems

## Some References



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Society for Industrial and Applied Mathematics, 2021

Other classic books:

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- ➡ Deans, *The Radon Transform and Some of Its Applications*, 1983
- ➡ Epstein, *Introduction to the mathematics of medical imaging*, 2008
- ➡ Kak & Slaney, *Principles of computerized tomographic imaging*, 1988
- ➡ Natterer, *The mathematics of computerized tomography*, 1986
- ➡ Natterer & Wübbeling, *Mathematical Methods in Image Reconstruction*, 2001